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## Amendments to the Claims

This listing of claims will replace all prior versions, and listings, of claims in the application:

## Listing of Claims:

- 1. (Currently amended) A computed tomography method comprising the steps of:
- a) generating, using a radiation source and a diaphragm arrangement which is arranged between the <u>an</u> examination zone and the radiation source, a fan beam which traverses an-the examination zone-on-and an object present therein,
- b) generating relative motions, comprising a rotation about an axis of
  rotation, between the radiation source and on the one-side and the examination zone or
  the object on the other side,
- c) acquiring measuring values which are dependent on the intensity of the radiation by means of a detector unit which detects, during the relative motions, the primary radiation from the fan beam and radiation which is coherently scattered in the examination zone or on the object, and
- d) reconstructing a CT image of the examination zone from the measuring values, during which reconstruction a back projection is carried out in a volume which is defined by two linearly independent vectors of the rotational plane and a wave vector transfer.
- (Currently amended) [[A]] The computed tomography method as claimed in claim 1, in which the back projection during the reconstruction step d) is performed along rays having a curved shape.
- (Currently amended) [[A]] <u>The</u> computed tomography method as claimed in claim 1, in which prior to the back projection in the reconstruction step d) the measuring values are multiplied by a first weighting factor which corresponds to the square of the

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distance between the scatter center, at which the detected ray was scattered, and the point of incidence of the scattered ray on the detector unit, and by a second weighting factor which corresponds to the reciprocal value of the cosine of the scatter angle.

- 4. (Currently amended) [[A]] The computed tomography method as claimed in claim 3, in which prior to the back projection in the reconstruction step d) all measuring values for each radiation source position are multiplied by a weighting factor which corresponds to the reciprocal value of the square of the distance between the radiation source position and the scatter center at which the detected ray was scattered.
- (Currently amended) [[A]] <u>The</u> computed tomography method as claimed in claim 1, in which the reconstruction step d) comprises the following steps:

one-dimensional filtering of the measuring values in the direction parallel to the rotational plane,

rebinning of the measuring values so as to form a number of groups, each measuring value measured by a detector element being associated with a line from the detector element to the radiation source position and each group comprising a plurality of planes which are parallel to one another and to the axis of rotation and in which a respective line fan is situated,

reconstruction of the distribution of the scatter intensity from the measuring values, a back projection then being carried out in a volume which is defined by two linearly independent vectors of the rotational plane and a wave vector transfer.

6. (Currently amended) A computer tomograph for carrying out the method claimed in-claim-1, comprising

a radiation source; and

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a diaphragm arrangement which is arranged between the <u>an</u> examination zone and the radiation source, in order to generate a fan beam which traverses anthe examination zone or an object present therein.

a detector unit which is coupled to the radiation source and comprises a measuring surface,

a drive arrangement for displacing an object present in the examination zone <u>with</u>
<u>respect to and</u> the radiation source relative to one another about <u>along</u> an axis of rotation
and/or parallel to the axis of rotation.

a reconstruction unit for reconstructing the distribution of the scatter intensity within the examination zone from the measuring values acquired by the detector unit[[]], and

a control unit for controlling a radiation source, the detector unit, the drive arrangement and the reconstruction unit in conformity with the steps a) to d) of claim 1.

- 7. (Currently Amended) A computer readable medium containing instructions for controlling [[a]] a control unit for controlling a radiation source, a diaphragm arrangement, a detector unit, a drive arrangement and a reconstruction unit of a computer tomograph so as to carry out a method comprising:
- a) generating, using a radiation source and a diaphragm arrangement which is arranged between the <u>san</u> examination zone and the radiation source, a fan beam which traverses anthe examination zone or an object present therein.
- b) rotating generating relative motions, comprising a rotation about an axis of rotation, between the radiation source <u>about on the one side and</u> the examination zone-or the object on the other side,
- c) acquiring measuring values which are dependent on the intensity of the radiation by means of a detector unit which detects, during the <u>rotation of the</u> <u>sourcerelative motions</u>, the primary radiation from the fan beam and radiation which is coherently scattered in the examination zone or on the object, and

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d) reconstructing a CT image of the examination zone from the measuring values, during which reconstruction a back projection is carried out in a volume which is defined by two linearly independent vectors of the rotational plane and a wave vector transfer.

8. (New) The method of claim 7, further including:

prior to the back projection, the measuring values are multiplied by a first weighting factor that corresponds to the square of the distance between the scatter center, at which the detected ray was scattered, and the point of incidence of the scattered ray on the detector unit, and by a second weighting factor that corresponds to the reciprocal value of the cosine of the scatter angle.

- 9. (New) The computed tomography method of claim 1, wherein the wave vector transfer is a function of a first distance between a detector element and a foot of the detector unit, a second distance between a scatter center and the foot of the detector unit, and an inverse wavelength of the coherently scattered radiation.
- 10. (New) The computed tomography method of claim 9, wherein the wave vector transfer is not a function of the scatter angle.
- 11. (New) The computed tomography method of claim 1, wherein the wave vector transfer is a function of  $A/(2D\lambda)$ , wherein A represents a distance between a detector element and a foot of the detector unit, D represents a distance between a scatter center and the foot of the detector unit, and  $\lambda$  represents the wavelength of the coherently scattered radiation

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(New) A computed tomography method, comprising:

generating, using a radiation source and a diaphragm arrangement arranged between an examination zone and the radiation source, a fan beam which traverses the examination zone:

generating a relative motion, comprising a rotation about an axis of rotation, of the radiation source about the examination zone and an object disposed therein:

acquiring measuring values which are dependent on the intensity of the radiation by means of a detector unit which detects, during the relative motion, the primary radiation from the fan beam and radiation which is coherently scattered in the examination zone; and

reconstructing a CT image of the examination zone from the measuring values, during which reconstruction a back projection is carried out in a volume which is defined by two linearly independent vectors of the rotational plane and a wave vector transfer, wherein the back projection is performed in the volume along rays having a curved shape.

- (New) The computed tomography method of claim 12, wherein the curved shape is a hyperbola.
- 14. (New) The computed tomography method of claim 12, wherein the hyperbola is a function of a distance between a scatter center and a foot of the detector unit.
- 15. (New) The computed tomography method of claim 12, wherein prior to the back projection the measuring values are multiplied by a first weighting factor which corresponds to the square of the distance between the scatter center, at which the detected ray was scattered, and the point of incidence of the scattered ray on the detector unit, and by a second weighting factor which corresponds to the reciprocal value of the cosine of the scatter angle.

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(New) A computed tomography system, comprising:

a detector that detects primary and scatter radiation traversing an examination

zone: and

a reconstructor that reconstructs measuring values indicative of the detected

radiation, wherein the reconstructor back projects the measuring values in a volume as a

function of a wave vector transfer that varies based on a difference between a scatter

center and a foot of the detector.

17. (New) The computed tomography system of claim 16, wherein the wave vector

transfer is a function of  $(1/\lambda)\sin(\theta/2)$ , wherein  $\lambda$  is the inverse wavelength of the scattered

radiation, and  $\theta$  is the scatter angle.

18. (New) The computed tomography system of claim 17, wherein the scatter angle

is a function of arctan(A/D), wherein A is a distance between the detector element and the foot of the detector unit and D is a distance between the scatter center and the foot of

the detector unit.

19. (New) The computed tomography system of claim 16, wherein an intensity of the

scatter is dependent exclusively on the scatter material.

20. (New) The computed tomography system of claim 16, wherein prior to the back

projection the measuring values are multiplied by a first weighting factor which

corresponds to the square of the distance between the scatter center, at which the detected ray was scattered, and the point of incidence of the scattered ray on the detector unit, and

by a second weighting factor which corresponds to the reciprocal value of the cosine of

the scatter angle.

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